



# Patient-specific 3D printed guides for repairing posterior root tears of the medial meniscus: A cadaveric study

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Meniscal root tears, classified as radial tears or avulsions up to 1 cm from the meniscal insertion, disrupt the circumferential fibers that convert axial loads into hoop stresses.<sup>[1]</sup> Medial posterior root tears reproduce the biomechanical consequences of total meniscectomy with increased contact pressure, reduced contact area, and higher risk of early osteoarthritis.<sup>[2-6]</sup> They are found in 7 to 9% of knee arthroscopies, mostly in the medial compartment, and their timely recognition is crucial, as delayed diagnosis or inadequate repair compromise joint

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## ABSTRACT

**Objectives:** The aim of this study was to evaluate the accuracy of tibial tunnel placement using patient-specific three-dimensional (3D)-printed guides for repairing medial meniscus posterior root tears designed from magnetic resonance imaging (MRI) scans.

**Materials and methods:** Five right fresh-frozen cadaveric knees underwent MRI scanning with 1-mm isotropic slices. For each specimen, custom guides were created to generate two transosseous tibial tunnels, with design based on anatomical landmarks including the medial tibial eminence (MTE) and the posterior cruciate ligament (PCL) insertion. Guide design was done using Rhinoceros software, segmentation of bone structures and soft tissues in 3D Slicer, and printing in polyamide. After arthroscopic repair, computed tomography scans and anatomical dissections were performed to measure the accuracy of tunnel placement relative to the native medial meniscus posterior root attachment (MMPRA), the MTE, and the PCL. Individual pre- and postoperative measurements were compared to verify anatomical accuracy, and pooled data from all knees were analyzed.

**Results:** Individual evaluation showed minimal differences between pre- and postoperative measurements, ranging from 0.00 to 0.09 mm. Pooled analysis revealed no significant differences in the measurements taken: PCL-MMPRA ( $p = 0.313$ ), MTE-MMPRA ( $p = 0.705$ ) or the width of MMPRA ( $p = 0.125$ ). The guides enabled precise and reproducible tunnel placement, with consistent targeting of the anatomical footprint. Each guide cost approximately €30, with a production turnaround time of less than one week.

**Conclusion:** Patient-specific 3D-printed guides enable the effective creation of two anatomically accurate tibial tunnels for medial meniscus posterior root repair. This approach offers a rapid and precise solution for anatomical restoration using MRI-guided planning.

**Keywords:** Additive manufacturing, knee arthroscopy, knee customized guides, meniscus posterior root tears repair, patient-specific instrument, 3D printing.

preservation.<sup>[7,8]</sup> Conservative treatment is reserved for patients with advanced cartilage degeneration (Kellgren-Lawrence Grade 3-4), advanced age, obesity, or significant comorbidities.<sup>[3,9,10]</sup>

Anatomical repair via transtibial tunnel techniques has become the gold standard surgical technique.<sup>[9]</sup> However, creating tibial tunnels that exit precisely at the native meniscal footprint still remains technically demanding. Existing surgical guides do not permit patient-specific planning, lack compatibility with variable tibial anatomy, and may result in malpositioned tunnels due to obstacles such as the tibial spines or femoral condyles. Misplacement has been linked to poor functional outcomes and rapid osteoarthritis progression.<sup>[11]</sup>

Three-dimensional (3D) printing has increasingly been used in orthopedic surgery to produce custom instrumentation for fracture fixation, oncology orthopedic reconstructions, osteotomies and arthroplasty.<sup>[12-19]</sup> However, no applications to date have addressed meniscal root repair with patient-specific guides. This represents a significant gap in the field, as tailored guides could improve surgical accuracy and reproducibility in this technically demanding procedure.

Although the main clinical challenge is the clear lack of individualized instruments for ensuring anatomical tunnel placement during medial meniscus posterior root repairs, in the present study, we aimed to evaluate the anatomical accuracy of tibial tunnels created using magnetic resonance imaging (MRI)-based, patient-specific 3D-printed guides designed to restore the medial meniscus posterior root via two transtibial tunnels.

## MATERIALS AND METHODS

This single-center, cadaveric study was conducted at University of Zaragoza (Spain), Department of Anatomy between December 2022 and December 2024. The study protocol was approved by the Aragón Ethics Committee (Date: 14.12.2022, No: PI22/529 TA).

In this study, we developed a cadaveric study in five right knees. Five right fresh-frozen cadaveric knee specimens with no evidence of prior injury, previous surgery, osteoarthritis, meniscal pathology, or ligament pathology were used. The cadaveric samples used in this study were obtained from a tissue bank and designated for medical research purposes. All specimens were kept at  $-20^{\circ}\text{C}$  and thawed for 24 h prior to preparation.

### Preoperative images and segmentation

Each specimen underwent MRI using a Magnetom Sola scanner (Siemens Healthineers, Munich, Germany) with 1-mm isotropic slice thickness and interval. This resolution provided adequate voxel uniformity ( $x = y = z$ ), enabling 3D reconstruction. Images were exported as Digital Imaging and Communications in Medicine (DICOM) files and processed in 3D Slicer version 5.2 software (The Slicer Community, MA, USA), using semi-automatic segmentation for bone structures.<sup>[20]</sup> Although 3D Slicer lacks automated tools for soft tissue segmentation from MRI, experienced users manually delineated structures such as the meniscus and posterior cruciate ligament (PCL) (Figure 1).

The anatomical landmarks identified for guide planning included:

- The native footprint of the medial meniscus posterior root attachment (MMPRA)
- The apex of the medial tibial eminence (MTE)
- The most superior tibial attachment of the PCL.

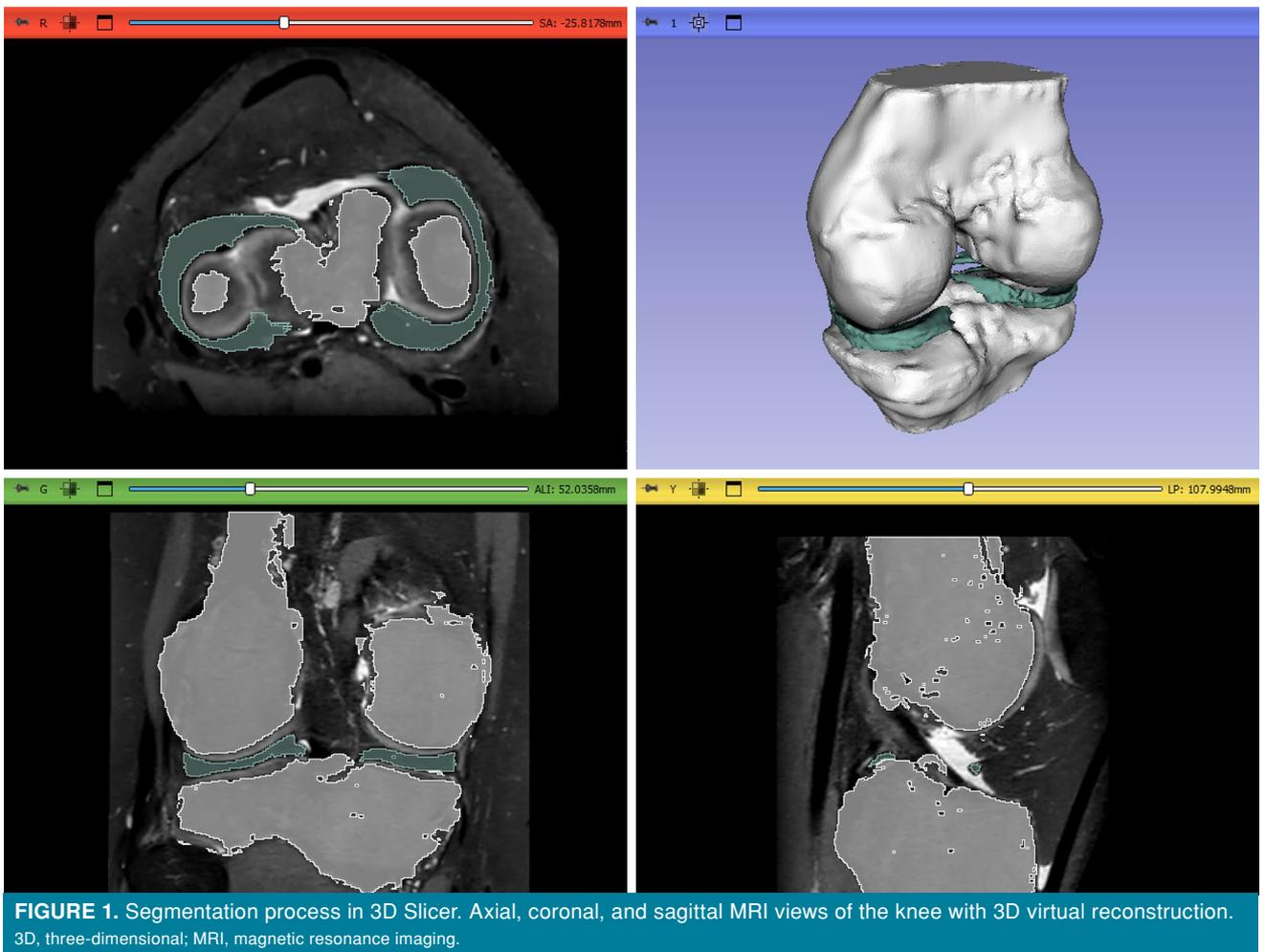
The coordinates of the MMPRA footprint were defined in three-dimensional space ( $x, y, z$ ), referenced from MTE and PCL. These coordinates were used for designing each guide.

### Guide design and manufacturing

A single customized guide was designed per knee using Rhinoceros CAD software (Rhino, Washington DC, USA). Each guide included a defined entry point on the anteromedial tibial cortex and two 3-mm bores to guide the creation of two parallel tibial tunnels converging at the MMPRA footprint (Figure 2). Tunnel exits were planned using the MRI-based 3D coordinates of the target footprint.

To assess tunnel orientation, three variants of the guide were virtually created per knee with angles of  $30^{\circ}$ ,  $45^{\circ}$ , and  $60^{\circ}$ , modifying only the external guide arm orientation (Figure 3). Although tunnel angles are largely defined by the external anatomy, this step ensured the selection of a configuration that avoided intra-articular impingement and optimized tunnel length and placement. After virtual evaluation, the  $60^{\circ}$  guide was selected for all specimens because  $30^{\circ}$  and  $45^{\circ}$  guides created short and horizontal tunnels.

All guides were printed in sterilizable polyamide (Figure 4) using an HP Jet Fusion 5200 printer (HP, CA, USA). Production cost was €30 per guide.



Manufacturing time from MRI acquisition to printed model was less than one week.

### Surgical procedure

Each procedure was performed with the specimen in the supine position and the knee flexed to 90°. Standard anterolateral and anteromedial portals were used for arthroscopy (Figure 5). The posterior horn of the medial meniscus was arthroscopically detached, and the 60° patient-specific guide was fixed on the anteromedial tibia. Two 2.7-mm tunnels were drilled, via the personalized guide, with an Acufex® trephine over a Kirschner wire. The target for tunnel exit was the MMPRA footprint, located posterior to the apex of the MTE and anteromedial to the tibial attachment of the PCL (Figure 6).

### Postoperative evaluation

All specimens underwent computed tomography (CT) examination after surgery. The CT images

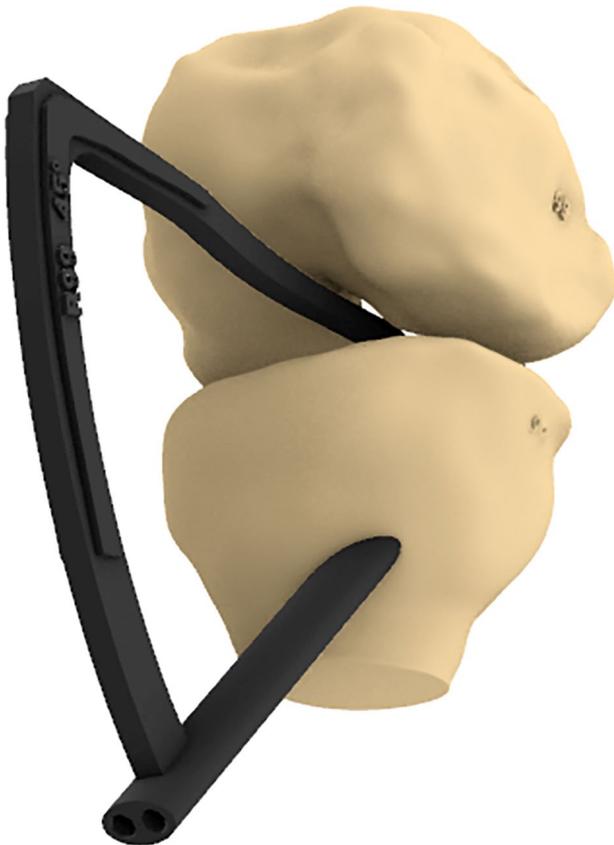
were obtained with an Aquilion™ 64 CT System (Toshiba Medical Systems, Tochigi, Japan) using 1-mm slice thickness.

Tunnel positions were analyzed in coronal, axial, and sagittal planes. The following parameters were measured (Figure 7):

- Distance from MTE apex to the midpoint between tunnel exits
- Distance from this midpoint to the most superior tibial attachment of the PCL
- Reinsertion width, calculated as the linear distance between both tunnels, including their full diameter.

All measurements were performed twice, and the mean values were recorded.

Subsequently, anatomical dissection was performed to directly visualize tunnel positioning relative to the PCL attachment. Digital calipers

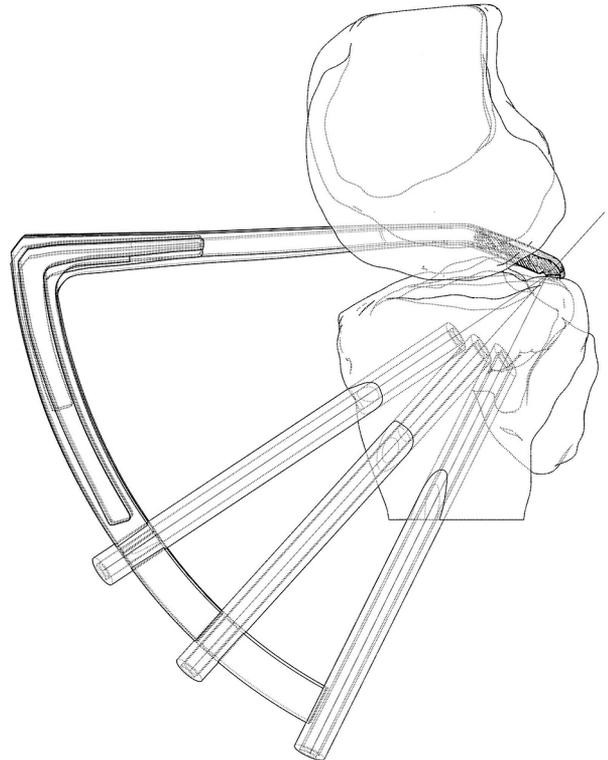


**FIGURE 2.** Virtual 3D reconstruction of a cadaveric knee with digitally planned customized guide.  
3D, three-dimensional.

(accuracy: 0.02 mm; resolution: 0.01 mm; UNE-EN ISO/IEC 17025 compliant) were used. All measurements were expressed in mm.

### Statistical analysis

Two complementary approaches were used to analyze the data. Firstly, each specimen was assessed individually by directly comparing its pre- and postoperative values for all anatomical references. This descriptive comparison allowed us to assess whether the surgical technique reproduced the anatomical footprint in each specimen. Secondly, to provide a formal statistical evaluation, all paired data were pooled and analyzed using the Wilcoxon signed-rank test, a non-parametric method appropriate for small sample sizes ( $n = 5$ ) and paired observations. Statistical analysis was performed using the Python version 3.11 software (Python Software Foundation, Wilmington, DE, USA) with the SciPy version 1.11 library. A  $p$  value of  $< 0.05$  was considered statistically significant.



**FIGURE 3.** Comparison of tunnel angles (30°, 45°, 60°) for guide optimization, based on 3D knee model.  
3D, three-dimensional.

## RESULTS

A total of five cadaveric knees were evaluated in this study. Measurements of the anatomical references were obtained pre- and postoperatively (Table I).

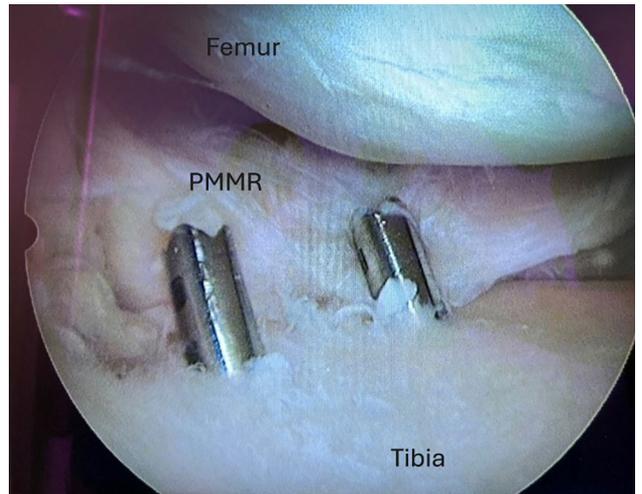
The accuracy of tunnel placement was evaluated by comparing the postoperative position of the tibial tunnel exits with the preoperatively planned coordinates derived from MRI (Table I).

Based on individual evaluation, the five knees showed almost identical values before and after the surgical procedure. The observed differences ranged between 0.00 and 0.09 mm (Table I), and none of them could be regarded as clinically relevant.

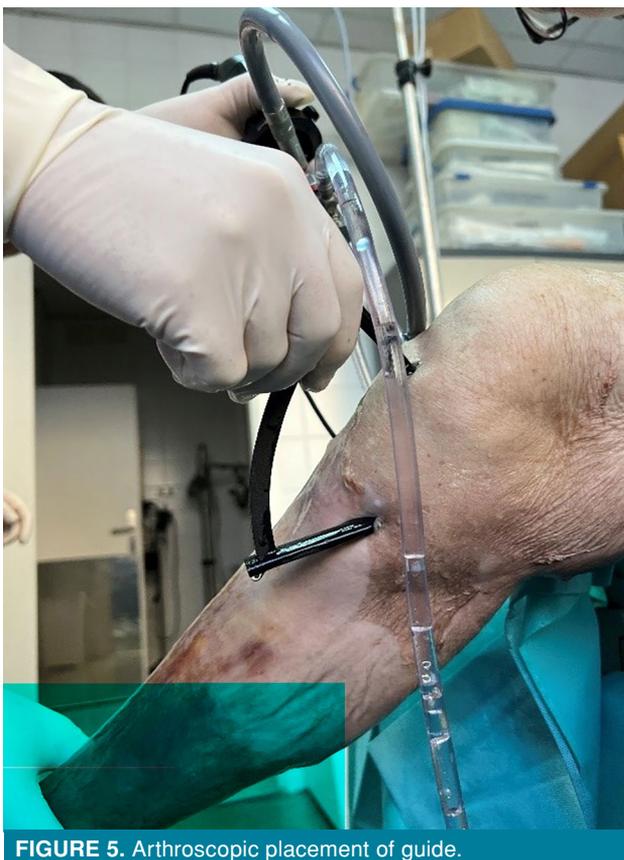
Based on pooled analysis of all specimens, no statistically significant differences were observed in PCL-MMPRA ( $p = 0.313$ ), MTE-MMPRA ( $p = 0.705$ ), or MMPRA reinsertion width ( $p = 0.125$ ). No significant differences were found in the statistical analysis between pre- and postoperative measurements for any of the three parameters evaluated.



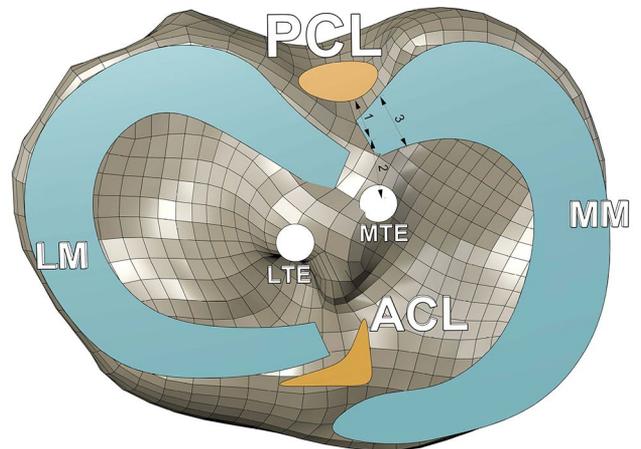
**FIGURE 4.** Final printed patient-specific guide in polyamide.



**FIGURE 6.** Tunnel drilling under direct visualization with 2.7-mm cannulated drills. PMMR, posterior medial meniscus root.



**FIGURE 5.** Arthroscopic placement of guide.



**FIGURE 7.** Schematic of planned tunnel positions and anatomical landmarks.

PCL, posterior cruciate ligament; LM, lateral meniscus; LTE, lateral tibial eminence; MTE, medial tibial eminence; ACL, anterior cruciate ligament, MM, medial meniscus. 1: distance from the midpoint of the MM insertion to the most superior tibial attachment of the PCL. 2: distance from MTE apex to the midpoint of the MM insertion. 3: insertion width of MM posterior root.

Taken together, both the individual comparisons and the pooled statistical test indicated that the technique restored the meniscal root to its anatomical position with high anatomical accuracy.

Across all specimens, the tunnel exits were visually confirmed to lie posterior to the apex of the MTE and anteromedial to the tibial PCL insertion, consistent with established anatomical descriptions.

**TABLE I**  
Pre- and postoperative anatomical measurements

Knee ID	Parameter	Preoperative (mm)	Postoperative (mm)	Difference (Post-Pre), (mm)
1	PCL-MMPRA	8.06	8.02	-0.04
	MTE-MMPRA	11.64	11.65	+0.01
	Reinsertion width	10.22	10.29	+0.07
2	PCL-MMPRA	8.55	8.52	-0.03
	MTE-MMPRA	11.82	11.84	+0.02
	Reinsertion width	10.61	10.70	+0.09
3	PCL-MMPRA	8.70	8.72	+0.02
	MTE-MMPRA	12.06	12.06	0.00
	Reinsertion width	10.71	10.70	-0.01
4	PCL-MMPRA	7.88	7.85	-0.03
	MTE-MMPRA	11.26	11.24	-0.02
	Reinsertion width	10.34	10.38	+0.04
5	PCL-MMPRA	8.75	8.76	+0.01
	MTE-MMPRA	12.32	12.30	-0.02
	Reinsertion width	10.92	10.99	+0.07

PCL, posterior cruciate ligament; MMPRA, medial meniscus posterior root attachment; MTE, medial tibial eminence; PCL-MMPRA, distance from the most superior tibial attachment of the PCL to the midpoint between tunnel exits. MTE-MMPRA: distance from MTE apex to the midpoint between tunnel exits. Reinsertion width, calculated as the linear distance between both tunnels, including their full diameter

Post-dissection assessment confirmed these positions, and no tunnel exit was observed to deviate outside the intended anatomical region.

The reinsertion width varied slightly among specimens, ranging from 10.29 to 10.99 mm, indicating the practical outcome of guide accuracy in replicating a broad-based contact area for meniscal healing. While this was not a direct surrogate for biological fixation strength, consistent spacing supported reproducibility in guide use.

## DISCUSSION

In this cadaveric study, we evaluated the anatomical accuracy of tibial tunnels created using MRI-based, patient-specific 3D-printed guides designed to restore the medial meniscus posterior root via two transtibial tunnels. Our study results demonstrated the feasibility of MRI-based, patient-specific 3D-printed guides for medial meniscus posterior root repair. In all cadaveric specimens, the guides enabled accurate and reproducible creation of two tibial

tunnels directed to the anatomical root footprint, confirming their technical viability.

Unlike most patient-specific instrumentation that relies on CT for bone segmentation, this approach shows that high-resolution MRI can provide sufficient detail for guide design, avoiding additional imaging.<sup>[15,18]</sup> Tunnel positioning was accurate, with exit points consistent with prior anatomical descriptions.<sup>[9,11,21]</sup> This accuracy is critical, as improper tunnel placement compromises meniscal function and increases the risk of PCL injury.<sup>[21]</sup>

Meniscal root tears alter tibiofemoral biomechanics, increasing contact pressure and reducing contact area.<sup>[3,4,9,22]</sup> Anatomical repair has been shown to restore biomechanics and improve joint loading.<sup>[3,9,23-26]</sup> The transtibial pullout repair, particularly the anatomical two-tunnel variation, is considered the gold standard.<sup>[2,3,9,10,22,27]</sup> Our guides were specifically developed to facilitate this technique, offering a practical single-device solution for double tunnel creation.

Compared to conventional guides, 3D-printed instruments offer customization, cost-effectiveness, and usability in cases with challenging anatomy or limited availability of commercial devices. While MRI-based design is more demanding than CT processing, it aligns with routine diagnostic practice and allows better identification of meniscal root attachments. The CT is still used postoperatively for tunnel verification, complemented by cadaveric dissection to assess PCL relationships. Overall, MRI-based 3D-printed guides represent a promising tool to improve accuracy, reproducibility, and accessibility in meniscal root repair, warranting further biomechanical and clinical validation.

Nonetheless, this study has several limitations. This study was conducted on cadaveric specimens without previous knee injuries. A relevant limitation, however, is that MRI was obtained from intact knees, and the lesion was artificially created afterwards, which may not fully replicate the clinical scenario of naturally occurring injuries. The sample size was also relatively small due to the high cost of every specimen and every image test, which limits the generalizability of the results. In addition, custom-made guides were designed from MRI images. Finally, all surgical procedures were performed by a single surgeon.

In conclusion, MRI-based, patient-specific 3D-printed guides provide a rapid and anatomically accurate method for double tibial tunnel creation in MMPRA repair. These findings support technical feasibility, reproducibility, and individualized anatomical adaptation, offering a solid basis for future clinical translation and further investigation into patient-specific instrumentation for soft-tissue knee surgery.

**Data Sharing Statement:** The data that support the findings of this study are available from the corresponding author upon reasonable request.

**Author Contributions:** C.M.H.: Idea/concept; C.M.H., M.D.S.: Design, writing the article; A.R.A., A.F.L.G.: Control/supervision; C.M.H., M.D.S., I.C.D.: Data collection and/or processing, analysis and/or interpretation; M.D.S., M.L.P., D.D.L.: Literature review; A.R.A., M.L.P., D.D.L., A.F.L.G., I.C.D.: Critical review.

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for language editing, and had no role in data analysis, interpretation, or the formulation of conclusions. All scientific content, data interpretation, and conclusions are the sole responsibility of the authors. The authors further confirm that AI tools were not used to generate, fabricate, or 'hallucinate' references, and that all references have been carefully verified for accuracy.

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